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Uber, III et al.

| [54] | PATIENT INFUSION SYSTEM FOR USE |
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| | WITH MRI |

[75] Inventors: Arthur E. Uber, III, Pittsburgh; Seid Waddell, Sarver; John Stulen; Jon E. Manley, both of Pittsburgh, all of Pa.

[73] Assignee: Medrad, Inc., Indianola, Pa.

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References Cited

U.S. PATENT DOCUMENTS

| 3,523,523 | 8/1970 | Reich et al 128/655 |
|-----------|--------|----------------------------|
| 3,812,843 | 5/1974 | Wootten et al 128/655 |
| 4,502,488 | 3/1985 | Degironimo et al 604/246 X |
| 4.695.271 | 9/1987 | Goethel 604/154 X |

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PATIENT INFUSION SYSTEM FOR USE WITH MRI

BACKGROUND OF THE INVENTION

1. Field of the Invention

This invention relates generally to the field of Magnetic Resonance Imaging (MRI) systems for generating diagnostic images of a patient's internal organs and more particu- 10 larly, this invention relates to improved MRI systems exhibiting decreased interference between the magnetic field used for producing diagnostic images and spurious magnetic fields created by ancillary equipment, such as the electric motors used for driving the pistons of the contrast media 15 injectors. Additionally, the system employs an improved communication link between an externally located system controller and the injection head control unit which is located within the electromagnetic isolation barrier of the magnetic imaging suite.

2. Description of the Related Art

It has become recognized that MRI systems require isolation from external sources of electromagnetic fields, if optimum image quality is to be obtained from MRI diagnostic procedures. Conventional MRI systems have typi- 25 cally employed some form of electromagnetic isolation chamber which is generally a room enclosed by copper sheeting or conductive mesh material that isolates the room from undesirable sources of electromagnetic radiation and the electromagnetic noise inherent in the atmosphere.

In order to realize the full benefit of the shielded room, these systems employ a controller for the contrast media injector portion of the system which is isolated from the media injector. Such isolation is effected to prevent undesirable electromagnetic radiation generated by the system controller from interfering with the signals used to create the magnetic resonance images.

The external, isolated location of the system controller creates various problems associated with the installation and operation of these systems. One such problem is the need to provide a communications link between the externally located controller and the contrast media injectors, without introducing extraneous electromagnetic radiation. That is, there is a need to provide electrical power supply lines for 45 operation of the contrast media injectors and the injector control circuitry while maintaining the integrity of the electromagnetic shield.

Previous attempts to solve these problems included drilling holes in the wall of the electromagnetic shield for 50 inserting the necessary lines or, alternatively, laying the lines under a shielded floor of the imaging room. These alternatives have proven to be less than optimum, since spurious radiation arose from the presence of the various supply cables within the shielded imaging suite. Additionally, MRI 55 systems which employed these solutions required substantial site dedication and were therefore not very portable.

Another problem associated with conventional magnetic resonance imaging systems is the interference which occurs between the high power magnetic field used for generating 60 the magnetic resonance image and the magnetic fields created by the electric motors which control the operation of the contrast media injection heads. The magnetic field generated by the magnet of the magnetic resonance imaging system is extremely powerful and adversely affects the 65 operation of the electric motors used in the injector head. Additionally, operation of the electric motors in close prox-

imity to the magnetic field used to generate the magnetic resonance image also has an adverse impact on the quality of the resulting image.

In conventional MRI systems, the injection head unit is

located adjacent to the patient being examined and the electric motors associated with the injection syringes are directly connected to the syringe pistons. Characteristically, the syringes and the drive motors have been mounted on the injection head unit. The close proximity of the electric motors to the magnetic field used for generating the magnetic resonance image typically resulted in a decrease in motor performance and the ability to control the electric motors used in the injector heads, as well as an overall decrease in system performance.

Accordingly, it is an object of the present invention to provide an improved magnetic resonance imaging contrast media delivery system having decreased interference between the magnetic field used to obtain the magnetic resonance image and the magnetic fields created by ancillary equipment.

It is a further object of this invention to provide an MRI system which minimizes the interference between fields created by the electric motors used to drive the contrast media injection plungers and the magnetic field used to generate the magnetic resonance image.

It is another object of the present invention to provide an MRI contrast media injection system having an improved communication link between the system controller and the injection control unit.

Numerous other objects and advantages of the present invention will be apparent from the following summary, drawings and detailed description of the invention and its preferred embodiment; in which:

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BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 is a block diagram outlining the functional design of the system; and,

40 FIG. 2 is a diagram illustrating the system of the present invention.

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SUMMARY OF THE INVENTION

The invention compromises an improved magnetic resonance imaging system which decreases the amount of electromagnetic interference that has heretofore been found within a MRI isolation suite while increasing the portability and ease of system installation. The invention reduces deleterious interaction between the imaging magnetic field and the magnetic field generated by the electric motors which control and operate contrast media injectors.

The system includes a master controller located externally of the shielded imaging room within which a contrast media injection head and a separate injection control unit are located. The system controller communicates with the head control unit via external and internal transceivers which form a communications link for traversing the electromagnetic isolation barrier of the imaging room.

In the preferred embodiment, this communication link is made through a window in the isolation room barrier. These windows are typically in the form of a glass laminate containing a conductive wire mesh, or alternatively, a window that is coated with a thin sheet of conductive material such as gold to maintain the shielding characteristics of the isolation room. The communications link consists of electromagnetic transceivers which operate in a frequency range

which permeates the window while maintaining the integrity of the isolation barrier. Infrared or electromagnetic energy in the visual range provide the best results. Alternatively, a fiberoptic communication link can be used to provide the communication link, since fiberoptics do not create electromagnetic radiation.

The present invention also incorporates a contrast media injection unit located within the shielded room which comprises separate contrast media injector head and injection head control unit. The contrast media injection head, and 10 specifically the syringe pistons are located in close proximity to the patient and consequently are located within the powerful magnetic field used to generate the magnetic resonance image. The head control unit which controls operation of the injector head is located from 10-15 feet 15 away from the injector head control unit. The head control unit incorporates electric motors to control and to operate the pistons of syringes used for the injection of patients. A non-rigid operating drive connects the electric motors and control unit to the syringe pistons located on the injection 20 head. In a preferred form, the drive connection can be by way of flexible shafts. Each flexible drive shaft forms a mechanical link between an electric motor located on the head control unit and a piston of the syringes on the injector head. Alternatively, a hydraulic system could be used to 25 control the piston of the injector head. In the preferred embodiment, the flexible drive shaft is manufactured from a non-ferrous metal such as hard brass. The distancing of the head control unit and drive motors from the injector head decreases the adverse effects that the imaging magnetic field 30 has on the electric motors of the injectors and conversely, the adverse affects of spurious electromagnetic radiation arising from operating of the electric motors used to control and operate the contrast media injectors is also reduced significantly.

DETAILED DESCRIPTION OF THE INVENTION

FIG. 1 illustrates an improved magnetic resonance imag- 40 ing system according to the present invention and is shown generally at 10. The MRI system includes a system controller 12 which incorporates a computer 14 and a battery charging unit 16. The system controller 12 is located externally of the imaging room 17, the imaging room being 45 shielded from electromagnetic interference by a shield 18. Isolation can be achieved by completely enclosing the room with copper sheet material or some other suitable, conductive layer such as wire mesh. Communication line 20, connects the system controller 12 with an external infrared/ 50 optical communications transceiver 22. The shielded imaging room 17 also incorporates a patient viewing window 24 in the shield 18 which allows an observer to view the room without breaching the electromagnetic shield 18. The window 24 can be formed by sandwiching a wire mesh material 55 (not shown) between sheets of glass or coating the window with a thin coating of conductive material such as gold (not shown) to maintain the continuity of the electromagnetic shield 18.

An infrared/optical communications transceiver 26 is 60 positioned internally of the imaging room 17 at the viewing window 24 opposite the external communications transceiver 22 such that the internal and external communications transceivers communicate with each other through the viewing window with no breach of the electromagnetic shield. A 65 communications link 28 located within the shielded area connects the internal infrared/optical transceiver with a

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